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(19) (CA) **CANADIAN PATENT** (12)

(54) ANESTHETIC SYSTEM

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ANAESTHETIC DEVICEBACKGROUND OF THE INVENTION

The present invention relates to devices utilizable in different types of breathing systems, such as those for administering anesthetic gases, or for the administration of oxygen to patients.

In recent years a number of improvements have been evolved for use in the practice of inhalation anesthetic administration. These improvements include: the two tube circle circuit disclosed in United States Patent No. 3,556,097; the unilimb device and the anesthesia breathing system disclosed in United States Patent No. 4,007,737; the anesthetic system described in the article entitled "A Streamline Anesthetic System" by J.A. Bain and W. E. Sporel, which appears in Volume 19, No. 4 at page 426 of the Canadian Anesthetic Society Journal (July 1972), and the tube device of which is disclosed in U.S. Patent No. 3,856,051 granted December 24, 1974; and the system described by Drs. S. Ramanathan, Chalou, and Turndorf in an article entitled "A Compact, Well-Humidified Breathing Circuit For the Circle System" which appeared in Volume 44, No. 3 commencing at page 238 of the March 1976 issue of Anesthesiology.

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1 Among such and other well-known breathing systems,
2 that most commonly used is probably the circle circuit,
3 originally introduced in 1926 and an improvement of which is
4 disclosed in Patent No. 3,556,097 mentioned above. The
5 principal problem in utilizing a circle circuit of such
6 design arises from the use of two flexible tubes. Such
7 tubes can impede the surgeon who may be confronted with
8 having to operate in the vicinity of the head and neck of
9 the patient. In addition, the same sized flexible tubes
10 used in a circuit system for adults, cannot be employed for
11 infants. Instead a miniturized pair of flexible tubes must
12 be utilized for the latter. While the rebreathing system
13 described by Drs. Bain and Sporel in the article, and his
14 pipe disclosed in said U.S. Patent No. 3,856,051, mentioned
15 above, have certain advantages from the standpoint of ease
16 in the application to the patient and handling, the parti-
17 cular circuit is not generally regarded as efficient with
18 regard to fresh gas economics during spontaneous breathing.
19 Nor would the fresh gas tube of the said patent support such
20 breathing. This pipe is, therefore, limited in its usage to
21 the Bain and Sporel rebreathing system which has not been
22 generally accepted to replace the circle circuit system.

23
24 In an effort to overcome the physical problems
25 presented by the use of two flexible tubes or hoses in the
26 manner illustrated in Patent No. 3,556,097, both the paten-
27 tee of Patent No. 4,007,737 and Drs. Ramanathan, Chalon, and
28 Turndorf have illustrated and described unilimb devices
29 utilizable in a circle circuit system.

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1 Although the unilimb devices thus suggested by
2 prior researchers in this field have offered advantages over
3 the two tube or hose system previously used in a circle
4 circuit system, there are certain critical aspects in such
5 prior unilimb devices which can present problems in certain
6 applications therefor and/or which may otherwise limit their
7 use to special situations. For example, although the uni-
8 limb of Patent No. 4,007,737 is designed to minimize dead
9 air space in a circle circuit breathing system, it does so
10 by providing two one way valves in the terminal connector
11 adapted for attachment to the mouth piece or other inlet
12 means to the patient's respiratory system. Since any mal-
13 function of either one-way valve could have a most serious,
14 if not fatal, consequence, it becomes highly desirable to
15 eliminate such valves altogether in this location. Further,
16 by providing spacers between the inner and outer tubes in
17 order to maintain them in a concentric disposition, the
18 unilimb of the last-mentioned patent can develop undesire-
19 able gas flow impediments when the tubes become twisted.
20

21 While the clinical report by Drs. Ramanathan et
22 al. does illustrate the use of a unilimb flexible tube or
23 hose system between the source of the gas and the patient,
24 insufficient details of the patient end of the device are
25 disclosed to enable one skilled in the art to determine its
26 exact physical structure.
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1 Prior art devices of these types, moreover, appear
2 to have been designed and utilizable only for particular
3 applications. Thus, for example, a unilimb device for a
4 circle circuit has had no utility in the rebreathing system
5 described by Drs. Bain and Sporel in the article heretofore
6 referenced. Conversely, no device specifically designed for
7 use in a rebreathing system, has heretofore been employable
8 in a circle circuit system.

9
10 Additionally, prior art devices have been struc-
11 tured for a particular application and with fixed physical
12 characteristics e.g. to provide a predetermined volume of
13 dead air space, thus limiting the use of the device to the
14 specific application for which the device may have been
15 designed. Hence, if, for example, it should become desire-
16 able in the circle circuit to provide more or less dead air
17 space than a given unilimb device is designed to provide, it
18 has been necessary heretofore to have a new unilimb device
19 designed and fabricated for such other specific application.

20
21 It has also been the observation of the present
22 inventor that such unilimb prior art devices as have hereto-
23 fore been described in any of the references, such as those
24 hereinabove mentioned, have not been found particularly
25 practicable from the standpoint of being readily manufactu-
26 rable at a reasonable cost. This would appear to be par-
27 ticularly the situation with respect to the device of Patent
28 No. 4,007,737 with its one-way valve system and spacers for
29 maintaining concentric disposition of the inner tube with
30 respect to the outer tube.

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1 If the cost of manufacturing such devices should
2 prove too great, there will be considerabl reluctance on
3 the part of hospitals and other potential users of the
4 devices to purchase the same, and particularly to discard
5 them where such discard might become necessary or desireable
6 after use with a patient which may have some type of commu-
7 nicable disease. Prior unilimb devices moreover have not
8 heretofore been constructed in such a manner as to be easily
9 disassemblable for cleaning sterilization or other type of
10 servicing.

11
12 Thus, the devices of the prior art have not proved
13 to be satisfactory from the standpoints of their fabrication,
14 their servicing, their disposability, their utility, nor
15 their adaptability for use in different systems, or for
16 different applications in the same system.

17
18 SUMMARY OF THE INVENTION

19
20 The present invention will be found to provide a
21 unilimb device which may be easily and inexpensively fabri-
22 cated for assembly or disassembly, and hence, is readily
23 servicable. It may be constructed for adaptation to uni-
24 versal applications, not only to satisfy different require-
25 ments for gas handling in the same system, but for use in
26 both the circle circuit system and the rebreathing system.

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Thus, the present invention provides a unilimb device for use in a breathing circuit wherein inspiratory gas from a source thereof is delivered through inlet means to a person's respiratory system, and expiratory gas exhaled by the person passes back through said inlet means, said device comprising:

A. first flexible tube means of such internal diameter as to pass the required volume of gas at the required rate from the source thereof to said inlet means to provide inspiration for the person, and said first flexible tube having a predetermined external diameter;

10

B. second flexible tube means enclosing most of the length of the first flexible tube means, said second flexible tube means being of such internal diameter greater than the predetermined external diameter of the first flexible tube means as to provide a sufficient cross-sectional area of passage between the first flexible tube means and the enclosing second flexible tube means to pass expiratory gas from the person at the required rate;

20

C. first terminal element means, said first terminal element means being generally tubular in configuration, short in length, and having one open nozzle end for communication with said inlet means, and an opposite open end including means for receiving and gripping a first end of the second flexible tube means and to dispose it close to the open nozzle end; said first terminal element means having a tubular wall defining a passage therethrough, a first end of the first flexible tube means being unattached to said second flexible tube means and said first terminal element means and extending axially toward said open nozzle end, and means within said first terminal element means for limiting the axial extension of said first end of the first flexible tube means toward said open nozzle end, to provide a

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1133350

passage for expired gas between said open nozzle and said first end of said first flexible tube means;

D. second terminal element means comprising a wall defining a cavity and first, second and third openings to said cavity;

10 said second terminal element means having a tubular extension defining said first opening including means for receiving and gripping the second end of the second flexible tube means, said tubular extension defining said first opening having an inner diameter larger than the outer diameter of said first flexible tube means;

 said second opening being disposed opposite said first opening, said second opening including means for receiving and securely gripping the second end of the first flexible tube means, when said first flexible tube means is inserted through said first opening, through said cavity into said receiving and gripping means thereby placing said first tubular means in direct communication with said second opening;

20 said third opening communicating with said cavity thereby placing said third opening in communication with said second flexible tube means through said cavity and said first opening.

 The invention comprises a pair of flexible gas conducting tubes, one being of a smaller diameter than the other and serving to conduct the inspiratory gas from a source thereof to inlet means for the patient's respiratory system. The larger flexible tube is disposed about the smaller tube and, through the space between the two tubes, may serve to conduct expiratory gas from such inlet means
30 back to a carbon dioxide absorber, or for other disposition.

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The two tubes extend between a pair of more rigid plastic terminals. One of such terminals may be provided with outer and inner tubular extensions to which one of the pair of corresponding ends of the larger and smaller tubes may be attached respectively, with the smaller tubular extension, placing the smaller tube in communication through an opening in the terminal with a hose from inspiratory gas source; and with the terminal providing a separate gas passage whereby the larger tubular member may be placed, through another opening in the terminal, in communication with a hose leading to the CO₂ absorber or other unit.

The other terminal may be short and tubular in configuration, having one end adapted for connection with the inlet means for the patient's respiratory system, and its other end adapted to receive the other ends of the two flexible tubes. The end of the larger tube may grippingly fit over or inside the other terminal end, and the end of the smaller tube may extend therein. An orificed transverse wall may be disposed between the two terminal ends and serve as a stop for the axial advance of the end of the smaller

D-6615

1133350

1 tube, thereby to prevent the inner tube from obstructing the
2 flow of expiratory air back through the larger tube. Because
3 of the proximity of the end of the smaller tube to the inlet
4 means the amount of dead space in the vicinity of the inlet
5 means to the patient's respiratory system, may be minimized.
6 The open ends of both the larger and smaller flexible tubes
7 are in direct communication with the nozzle leading to the
8 inlet means to the patient's respiratory system, as well as
9 with each other. Since the pressure of the gas arriving
10 through the smaller tube will always be in excess of the
11 pressure of the gas being carried away by the larger tube,
12 and because the one-way valves are already provided by the
13 anesthesia machine, no one-way valve has been found to be
14 necessary at the outlet of the inner tube, or the entrance
15 of the outer tube. Even when the patient exhales back through
16 the nozzle, the expiratory gas will be carried away between
17 the walls of the larger and smaller tubes.

18
19 While the device in a circle circuit system thus
20 provides a minimum of dead space, a requirement particularly
21 important in the administration of oxygen to infants, it is
22 also part of the present invention to provide telescoping or
23 adapter elements for either or both of the terminals whereby,
24 paradoxically, dead space may be increased for situations
25 where the level of the carbon dioxide in a patient may become
26 abnormally low, as for example, where patients may be re-
27 ceiving prolonged artificial ventilation. By sliding out
28 the telescoping tubular extensions, the circuit may readily
29 be adapted to provide adequate dead space to enable the
30 patient's carbon dioxide level to be regulated over a wide
31 range, thereby facilitating the maintenance of normocapnia
32 ///

D-6615

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1 during anesthesia and mechanical ventilation, when appro-
2 priate.

3

4 It is also a feature of the present invention that
5 the second terminal, which may normally be connected to the
6 source of gas, and the carbon dioxide absorber, may be modi-
7 fied in a number of ways by the use of a plug and an adapter,
8 to increase dead space in a circle circuit. Additionally,
9 by connecting a bag or a respirator, or a one-way valve, to
10 the opening in the terminal which would normally be in commu-
11 nication with a carbon dioxide absorber in a circle circuit
12 system, the device may be adapted to a rebreathing or non-
13 rebreathing circuit for use in transporting a patient away
14 from an operating room during recovery or when adequate
15 anesthetic machines are not readily available.

16

17 Because the components of the device of the present
18 invention are relatively simple to construct and may be
19 manufactured as separate items, they may be easily assembled
20 into the complete unilimb device, and any one of the compo-
21 nents may be quickly replaced should such replacement become
22 necessary. Additionally, since the several components may
23 be readily detached from the other components, each of the
24 components may be easily cleaned and sterilized. Also,
25 because the cost of fabricating the several components is
26 not great, any or all of the components may be simply be
27 disposed of after any use thereof, as for example, by a
28 patient having a contagious disease or a communicable virus.

29

30 While it is contemplated that the inner tube shall
31 be used as the inspiratory limb, and the outer tube as the
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D-6615

1133350

1 expiratory limb in order to avoid obstruction due to water
2 condensation of the exhaled gases which may occur after
3 prolonged artificial ventilation, it would be possible to
4 reverse the connections without hypercarbia and hypoxia
5 presenting immediate hazards to the patient.
6

7 The device of the present invention may thus be
8 adapted for use in any of the several presently used breathing
9 systems in order to utilize the most desirable features
10 of such circuit for any particular application. In
11 other words, the same unilimb device may be utilized either
12 in a circle circuit, or as a re-breathing circuit, or a non-
13 rebreathing circuit, a pediatric circuit with a minimum dead
14 space, or to provide greatly augmented dead space in any of
15 such circuits to regulate arterial carbon dioxide. Moreover,
16 the device has proven to be extremely reliable and affords
17 safe institution of spontaneous, assisted or controlled
18 ventilation. This results particularly from the elimination
19 of valves in the terminal and the need for maintaining concentricity
20 of the tubes by spacers or other means.
21

22 BRIEF DESCRIPTION OF THE DRAWINGS

23

24 In the accompanying drawings:

25 Figure 1 illustrates, in perspective view, a typical
26 conventional dual tube circle circuit;

27 Figure 2 is a schematic view of the circle circuit
28 of Figure 1;

29 Figure 3 is a longitudinal cross-section of the
30 preferred embodiment of the device of the present invention;
31 ///

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1 Figure 4(a) is a section on the line a-a of Figure
2 3;

3 Figure 4(b) is a section on the line b-b of Figure
4 3;

5 Figure 4(c) is a section on the line c-c of Figure
6 3;

7 Figure 4(d) is a section through the line d-d of
8 Figure 3;

9 Figure 4(e) is a section on the line e-e of Figure
10 3;

11 Figure 4(f) is a section on the line f-f of Figure
12 3;

13 Figure 5 is a front view of the transverse wall
14 element 29 shown in Figure 3;

15 Figure 6 is a schematic view of a circle circuit
16 of Figure 2 in which the device of Figure 3 has been substi-
17 tuted for the two hose arrangement of Figures 1 and 2;

18 Figure 7(a) is a longitudinal section of a modified
19 form of the terminal element shown in the left-hand side of
20 Figure 3;

21 Figure 7(b) is a front view of the modified trans-
22 verse wall element 30 and surrounding elements shown in
23 Figure 7(a);

24 Figure 8(a) is also a longitudinal section of the
25 terminal element shown in the left-hand side of Figure 3,
26 but illustrating a modification in the end of the inner
27 tube;

28 Figure 8(b) is a longitudinal section of a still
29 further modification of the end of the inner tube;

30 Figure 9(a) is a longitudinal section of the
31 terminal element shown on the left-hand side of Figure 3,

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1 but illustrating the substitution for the transverse wall in
2 Figure 3 of a screen type wall, and a different disposition
3 of the inner tube;

4 Figure 10(a) is a longitudinal section of the
5 terminal shown on the left-hand side of the Figure 3, in a
6 further modified form;

7 Figure 10(b) is a view taken on the line aa of
8 Figure 10(a) looking in the direction of the arrows;

9 Figure 11(a) is a longitudinal section of the
10 terminal shown on the left-hand side of the Figure 3 in a
11 still further modified form;

12 Figure 11(b) is a view taken on the line a-a of
13 Figure 11a looking in the direction of the arrows;

14 Figure 12 is a longitudinal section of a modified
15 form of the terminal shown on the right-hand side of Figure
16 3;

17 Figure 13 is a longitudinal section of the termi-
18 nal shown on the right-hand side of Figure 3, but with base
19 connections thereto;

20 Figure 14 is a longitudinal section similar to
21 Figure 3, but illustrating a modification of, and addition
22 to, the terminal shown on the right-hand side of Figure 3;

23 Figure 15 is a schematic view of the circuit in
24 which the embodiment of the invention illustrated in the
25 Figure 14 may be utilized;

26 Figure 16 is a sectional-view of still further
27 modification of, and addition to, the terminal illustrated
28 on the right-hand side of Figure 3.

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1133350DESCRIPTION OF THE PREFERRED EMBODIMENTS

1 Referring to Figure 1 of the drawings, a typical
2
3 circle circuit includes a source of gas 1, conduit means 2
4 extending therefrom, and a carbon dioxide absorber 3 which
5 receives expiratory gas through a conduit 4. Reprocessed
6 gas moves out through the outlet 5 after having passed
7 through the carbon dioxide absorbing granule 6. As the
8 reprocessed gas moves out of the outlet 5, it joins fresh
9 gas from the source 1 as the fresh gas is arriving through
10 the conduit 7, and the merged gases then pass through the
11 one-way inspiratory valve 13 and the flexible hose 9 into
12 the common inlet-outlet pipe 11, as inspiratory gas to the
13 inlet means (not shown) to the patient's respiratory system.
14 The expiratory gases return through the inlet pipe 11, but
15 then pass back through the return hose 10, one-way expira-
16 tory valve 14, past the reservoir bag 12 and into the carbon
17 dioxide absorber 3 through the inlet for reprocessing. This
18 system is shown schematically in Figure 2.
19
20

21 The device of the present invention is intended to
22 replace the two hoses 9 and 10, and the inlet-outlet pipe 11
23 of the circle circuit thus illustrated in Figures 1 and 2,
24 and briefly described above. The inspiratory tube 21 is
25 extended through the expiratory tube 22. The difference in
26 the diameters of these two tubes is such that a sufficient
27 volume of expiratory air may pass between the outer wall of
28 the inner tube 22 and the inner wall of the outer tube 21.
29 The latter desirably may be constructed of plastic, as a
30 corrugated tube, while the inner tube 22 preferably is extruded
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D-6615

1133350

1 of a vinyl type material. These two tubes are separately
2 fabricated, so that when the device of the present invention
3 is to be assembled, the smaller tube 22 is simply pushed in
4 and through the outer tube 21 until the leading end of the
5 tube 22 appears at the other end of the corrugated outer
6 tube 21.

7
8 As may be seen in Figure 3, two corresponding ends
9 22' and 21a of the inner tube 22 and outer tube 21 are dis-
10 posed in and about a terminal element 23, respectively.
11 This element 23 may be generally tubular in configuration,
12 with a tapered nozzle end 23a for connection with the inlet
13 means to the patient's respiratory system. The external
14 diameter of the opposite cylindrical end 23b of the ter-
15 minal element 23 is such as to enable the uncorrugated end
16 21a of the tube 21 to be force fitted thereover. A trans-
17 verse wall 29, preferably orificed in the manner shown in
18 Figure 5, with the orifices 29', may serve as a stop to
19 prevent the end 22' of the tube 22 from extending into the
20 opening in the nozzle end portion 23a of the terminal ele-
21 ment 23 and thereby block the flow of expiratory air back
22 into the expiratory air passage 21c, but permitting such end
23 22' to be disposed as close as possible to the opening in
24 the nozzle and portion 23a.

25
26 The opposite ends 21b and 26 of the tubes 21 and
27 22 respectively, are connected to a second terminal element

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1 24. This second terminal element 24, in the embodiment
2 shown in Figure 3, comprises a wall or housing 24a which
3 defines three openings--24b, 27 and 28, and a cavity 24c,
4 and includes a tubular extension portion 24d. The opening
5 24b may be coaxial with the opening 28. The end 21b of the
6 tube 21 may be forced fitted over a sleeve 21", which itself
7 is slipped over the tubular extension 24d, but only after
8 the end 26 of the smaller inner tube 22 is first inserted
9 through the opening 24b and passed through the cavity 24c
10 and into a smaller receiving area 24e, into which the end 26
11 may be force fitted, thereby placing it in direct communi-
12 cation with the opening 28. After the end 26 of the inner
13 tube 22 has thus been securely inserted in and gripped by
14 the wall-defining the area 24e, and the outer tube end 21b
15 has been attached over the tubular extension 24d in the
16 manner heretofore described, the unilimb device of the
17 present invention is ready for connection into a circle
18 circuit system of the type shown in Figures 1 and 2, in the
19 manner illustrated in Figure 6. Thus, the opening 27 may be
20 connected as at 14 in Figure 2, and the opening 28 is con-
21 nected to the inspiratory air line as at 13 in Figure 2.
22 The terminal element 23 then substitutes for the inlet-out-
23 let 11 shown in Figures 1 and 2. Thereby, there are elimi-
24 nated from the circuit the cumbersome double hose 9, 10, and
25 Y-pipe connection shown at 11a in Figure 1. The manner in
26 which this substitution thus appears is illustrated in
27 Figure 6. While this device of the present invention in the
28 embodiment illustrated in Figure 3 provides a minimum of
29 dead air space between the end 22' of inner tube 22 and the

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D-6615

1133350

1 opening in the nozzle 23, which is connected to the inlet
2 means (not shown) to the patient's respiratory system;
3 should a small increase in such dead space be required or
4 desirable in any situation, the same may be readily ob-
5 tained by sliding the sleeve 21" axially to the left along
6 the tubular extension 24d. Thereby, the corrugated outer
7 tube 21 and terminal 23 are also displaced axially to the
8 left relative to the inner tube 21, with the result that the
9 end 22' becomes disposed toward the right further away from
10 the opening in the nozzle end portion 23a of the terminal
11 23, to increase the dead space between said opening and end
12 22'.
13

14 It will be readily appreciated by those persons
15 skilled in the art that the inspiratory air from the source
16 1, as supplemented by air from the carbon dioxide absorber
17 3, is brought to the inlet means (not shown) of the patient's
18 respiratory system through the opening 28, the tube 22, and
19 the terminal element 23. Expiratory air on the other hand,
20 passes back from the patient into the terminal element 23,
21 where it is diverted around the incoming inspiratory air at
22 the end 22' of the inner tube 22, and into the passage of
23 21c between the outer corrugated tube 21 and the inner tube
24 22. This expiratory air is then brought back through the
25 terminal element 24 via the passage defined by the tubular
26 extension 24d, the cavity 24c, and the opening 27, from
27 whence it is carried back past the reservoir bag 12, and
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1 into the carbon dioxide absorber 3 for reprocessing and
2 ultimate return with fresh inspiratory gas.

3
4 It will be readily appreciated that in this
5 particular embodiment shown in Figure 3, there is provided
6 in the terminal element 23, a minimum of dead space. While
7 the device as illustrated in Figures 3-5 is to be preferred,
8 at least for those applications where a minimum of dead
9 space may be desired, other configurations of the terminal
10 element and two tube ends may also be utilized.

11
12
13 In the embodiment of the terminal element
14 illustrated in Figures 7(a) and 7(b), the orificed trans-
15 verse wall 29 of the Figure 3 embodiment is omitted, and a
16 plurality of radially extending spacers 30 secured to the
17 cylindrical wall portion 23 are provided to support the end
18 22' of the tube 22 in coaxial alignment with the terminal
19 element 23, and to limit the distance that the tube end 22'
20 may extend toward the nozzle opening.

21 In the further embodiment of the terminal element
22 illustrated in Figures 8(a) and 8(b), the only modifications
23 over that of Fig. 3 lies in providing the orifices 31 or
24 serrations 31' in the end 22' of the inner tubular member
25 22.

26
27 In the still further embodiment of the invention
28 illustrated in Figures 9(a) and 9(b), there is substituted
29 for the transverse wall 29 of the Figure 3 embodiment, a
30 screen-like member 29', and the inner inspiratory air tube

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D-6615

1133350

1 is brought into the terminal element 23 along the side of
2 the outer tubular member 21.

3
4 In the still further embodiment of the invention
5 illustrated in Figures 10(a) and 10(b), there is substituted
6 for the transverse wall 29 in the Figure 3 embodiment, an
7 orificed transverse annular wall 32', having a coaxial tubu-
8 lar extension 32 which serves to receive and limit the axial
9 incursion of the end 22' of the inner tube 22. Additionally,
10 the inner wall 23b' is configured to provide a counter bore
11 type recess 23b'' to receive the radiating flange 32' which
12 constitutes a transverse wall referred to above. This
13 flange or wall 32' is punctured with a ring of orifices 33
14 for passage of expiratory air back into the passage 21c
15 defined by the inner wall of the outer tube 21 and the outer
16 wall of the inner tube 22.

17
18 In the last alternate embodiment of the terminal
19 element 23, illustrated in Figures 11(a) and 11(b), it will
20 be seen that this is quite similar in configuration to the
21 embodiment of Figures 10(a) and 10(b), the difference being
22 that the axially extending orifices 33, shown in Figures
23 10(a) and 10(b) have been eliminated from the transverse
24 wall-flange 32. In place of said axially extending orifices
25 33, a series of orifices 33' have been provided in the tubu-
26 lar extension 32, thereby to permit the expiratory gas to
27 pass into the passage 21c.

28
29 Figure 12 illustrates a possible different confi-
30 guration for the right-hand terminal element shown in Figure

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1 3, and Figure 13 illustrates the manner in which tubes 34
2 and 35 may be inserted into the openings 27 and 28 respec-
3 tively, to place this element in communication with the
4 carbon dioxide absorber 3 and the gas source 1 in a circuit
5 such as is illustrated in Figure 6..
6

7 In the further embodiment of the invention illus-
8 trated in Figures 14 and 15, it will be noted that the basic
9 device illustrated in Figure 3 is employed, but it has been
10 modified to the extent of having had its opening 27 closed
11 by a plug 34', and instead of having the end of a connector
12 tube 35 inserted into the opening 28, as illustrated in
13 Figure 13, an interfitting end 37 of an extension adapter 38
14 is pressed into the opening 28. This adapter, however, does
15 not continue the separation of the inspiratory and expira-
16 tory air passages in the manner accomplished by the terminal
17 element 24, as illustrated in Figures 3, 12 and 13. Instead,
18 the extension adapter 38 defines a single cavity 39, into
19 which there are three openings 40, 41, and 42. Opening 40
20 is placed in direct communication with the inner tube 22.
21 The oppositely disposed opening 41 is placed in communica-
22 tion with the tube 35 from the source of gas 1 and repro-
23 cessed gas from the CO₂ absorber 3; while the third opening
24 42 is placed in communication through the elbow 43 and the
25 hose 36 with the carbon dioxide absorber 3, in the manner
26 shown in the schematic diagram of Figure 15. This adapta-
27 tion of the present invention, in effect, provides an exten-
28 sive dead space for use in situations where it is desired to
29 increase the level of carbon dioxide in the patient's respira-
30 tory system.
31 ///

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1133350

1 In th further adaptation illustrated in Figure
2 16, the plug 34''serves to close off the opening 28 and
3 h nce, the end of the inner tube 22. The circle circuit
4 illustrated in Figure 16, in this alternative embodiment, is
5 connected by the adapter 38' to the opening 27' and the two
6 hoses 35 and 36. By this adaptive embodiment, it may be
7 seen that the circle circuit is provided with more extensive
8 dead space by employing only the outer tube 21 not the inner
9 tube 22.

10
11 From the foregoing it will be readily appreciated
12 by those skilled in the art that the device of the present
13 invention may not only be employed effectively in a circle
14 circuit breathing system to provide a minimum of dead space
15 but it may be readily adapted to provide greatly augmented
16 dead space in such a system, and also may be adapted for use
17 in various other presently known breathing systems. The
18 device may be readily assembled from its basic components
19 and, since it contains no moving valve parts, it is
20 completely safe and reliable. Because of the simplicity of
21 the structures of its components, it is easy to disassemble
22 for cleaning and sterilization. Moreover, since its compo-
23 nents may be inexpensively manufactured, any of such compo-
24 nents, or even the entire device may be disposed of after
25 usage in certain situations, without great economic loss.
26

27 What is claimed is:
28
29
30
31
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1133350

THE EMBODIMENTS OF THE INVENTION IN WHICH AN EXCLUSIVE PROPERTY OR PRIVILEGE IS CLAIMED ARE DEFINED AS FOLLOWS:

1. A unilimb device for use in a breathing circuit wherein inspiratory gas from a source thereof is delivered through inlet means to a person's respiratory system, and expiratory gas exhaled by the person passes back through said inlet means, said device comprising:

A. first flexible tube means of such internal diameter as to pass the required volume of gas at the required rate from the source thereof to said inlet means to provide inspiration for the person, and said first flexible tube having a predetermined external diameter;

B. second flexible tube means enclosing most of the length of the first flexible tube means, said second flexible tube means being of such internal diameter greater than the predetermined external diameter of the first flexible tube means as to provide a sufficient cross-sectional area of passage between the first flexible tube means and the enclosing second flexible tube means to pass expiratory gas from the person at the required rate;

C. first terminal element means, said first terminal element means being generally tubular in configuration, short in length, and having one open nozzle end for communication with said inlet means, and an opposite open end including means for receiving and gripping a first end of the second flexible tube means and to dispose it close to the open nozzle end; said first terminal element means having a tubular wall defining a passage therethrough, a first end of the first flexible tube means being unattached to said second flexible tube means and said first terminal element means and extending axially toward said open nozzle end, and means within said first terminal element means for limiting the axial extension of said first end of the first flexible tube means toward said open nozzle end to provide a

1133350

passage for expired gas between said open nozzle and said first end of said first flexible tube means;

D. second terminal element means comprising a wall defining a cavity and first, second and third openings to said cavity;

10 said second terminal element means having a tubular extension defining said first opening including means for receiving and gripping the second end of the second flexible tube means, said tubular extension defining said first opening having an inner diameter larger than the outer diameter of said first flexible tube means;

said second opening being disposed opposite said first opening, said second opening including means for receiving and securely gripping the second end of the first flexible tube means, when said first flexible tube means is inserted through said first opening, through said cavity into said receiving and gripping means thereby placing said first tubular means in direct communication with said second opening;

20 said third opening communicating with said cavity thereby placing said third opening in communication with said second flexible tube means through said cavity and said first opening.

2. The device as defined in claim 1 wherein said means for limiting the axial extension of the first flexible tube means comprises a transverse orificed wall proximate the open nozzle end.

3. The device as described in claim 1 wherein the first end of the first flexible tube means is orificed radially to provide gas passages directly between the end area of the first flexible tube means and the gas passage about said first flexible tube means end and defined by the inner wall of said first terminal element means.

1133350

4. The device as described in claim 2 wherein the orificed transvers wall is comprised of screening.

5. The device as described in claim 1, wherein the axes of the second and third openings in the second terminal element means intersect each other at other than a right angle.

6. In combination with the device as described in claim 1, means to plug the second opening in the second terminal element means thereby to close off the second end of the first flexible tube means, and adapter means, said adapter means having one end interfittable into the third opening in the second terminal element means, said adapter means defining a gas passage extending from its said one end and two further openings to the last said gas passage, each of said openings being connectible to conduits in a breathing circuit.

7. In combination with the device as described in claim 1, means to plug the third opening in said second terminal element means thereby to close the same to any gas passage therethrough, and adapter means, said adapter means having one end interfittable into the second opening in the second terminal element means, said adapter means defining a gas passage extending from its said one end and two further openings to the last said gas passage, each of said openings being connectible to conduits in a breathing circuit.

8. The device as described in claim 1 wherein sleeve-like means are interposed radially between the tubular extension of the second terminal element means and the second end of the second flexible tube means, the last said end being fixedly fitted about a portion of said sleeve-like means and the latter being axially slidable relative to said tubular extension.

1133350

9. The device as described in claim 1 wherein sleeve-like means are interposed radially between the tubular extension of the second terminal element means and the second end of the second flexible tube means, the last said end being fixedly fitted about a portion of said sleeve-like means, and the latter being rotatable relative to said tubular extension.



ABSTRACT OF THE DISCLOSURE

This application discloses a unilimb device of universal application to different types of breathing systems. The device comprises two gas carrying tubes, one within the other, the corresponding ends of the tubes being within two common terminal elements. One of the terminal elements provides for two separate passages, each being connectable, one to a source of gas, and the other for disposition of the expiratory gases. The other terminal element includes a nozzle end for connection to the inlet for the patient's respiratory system, with the opposite end serving to receive the other ends of the two flexible tubes and to provide short passages to the nozzle to minimize dead air space. Provision may be made for telescoping each terminal element, and the inlet element may be provided with a member for extending or adapting it to different breathing systems.

1133350

8-1

Fig. 1

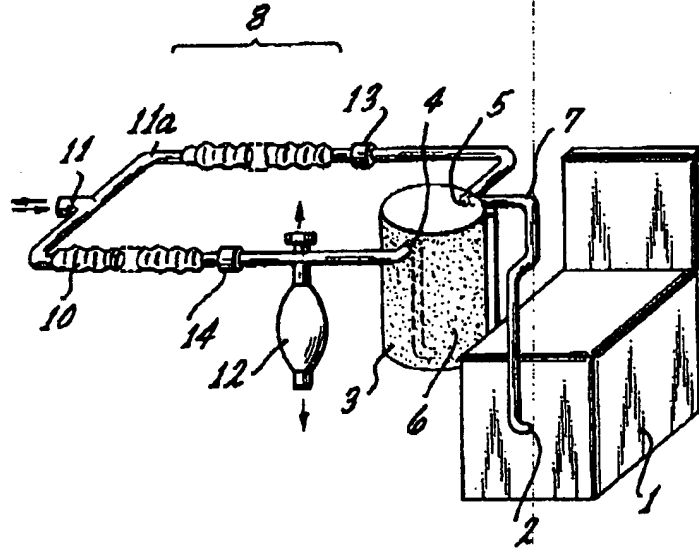
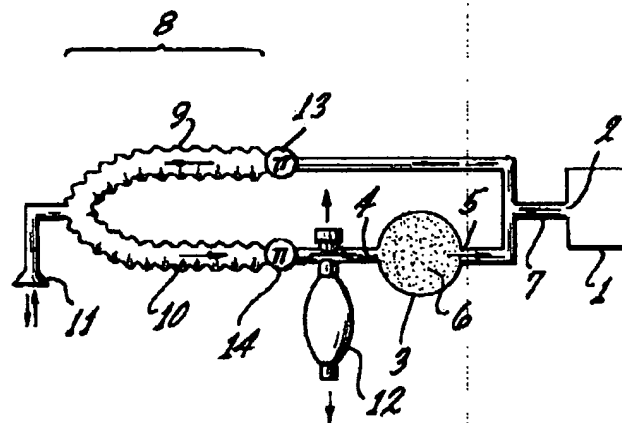


Fig. 2



Scott & Lydon

1133350

8-2

FIG. 3

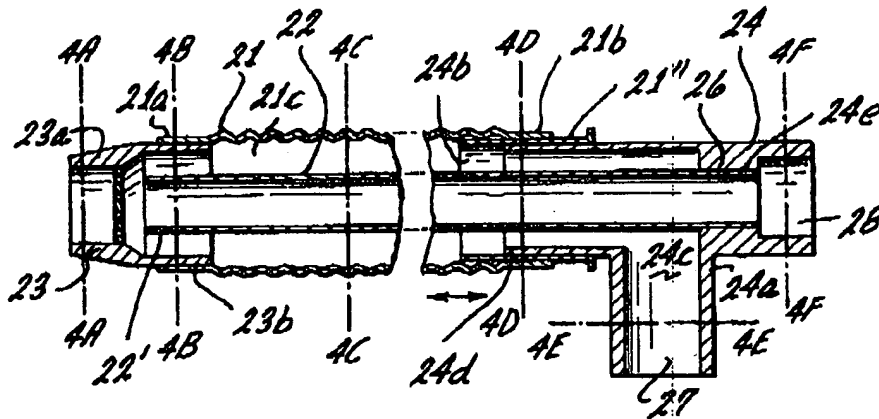


FIG. 4a

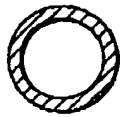


FIG. 4b

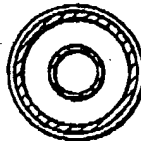


FIG. 4c

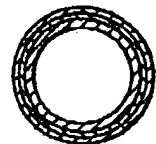
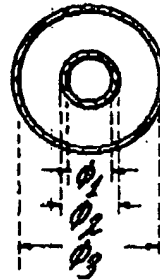


FIG. 4d

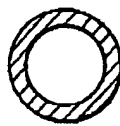


FIG. 4e,f

Scott & Lyman

1133350

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Fig. 5

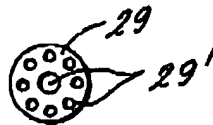
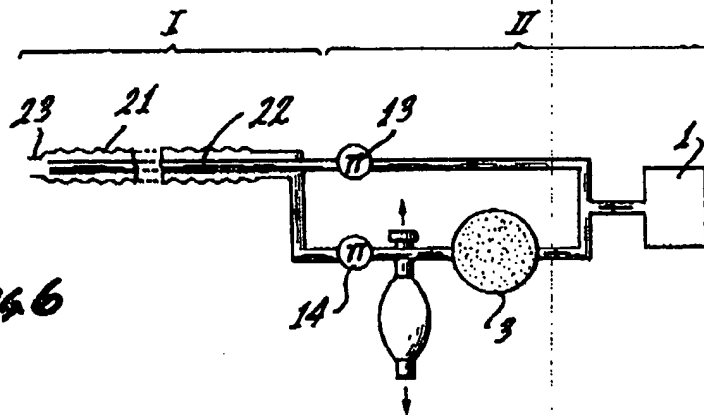


Fig. 6



Scott & Lyon

1133350

8-4

Fig. 7a

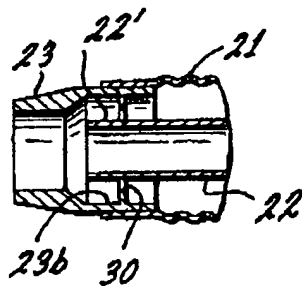


Fig. 7b

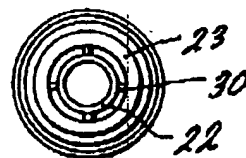


Fig. 8a

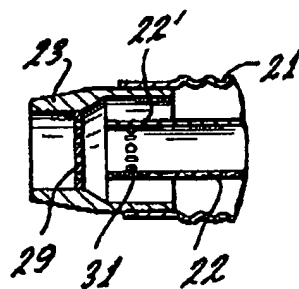


Fig. 8b

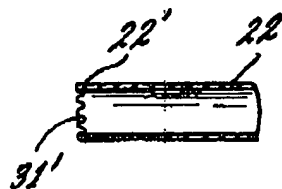


Fig. 9a

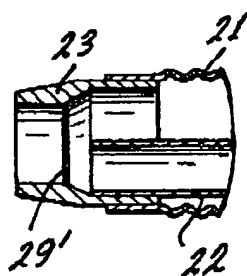
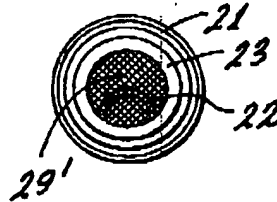


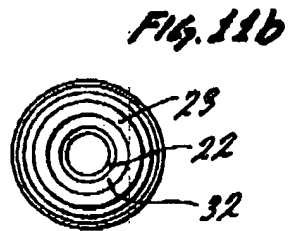
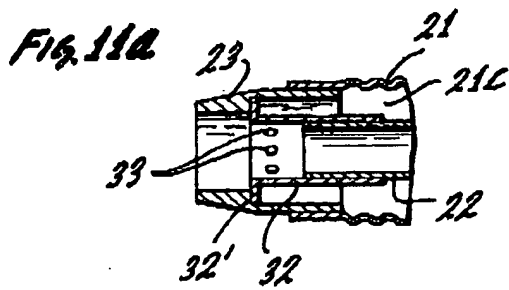
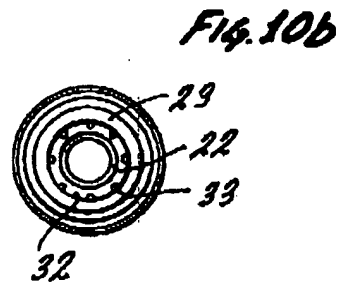
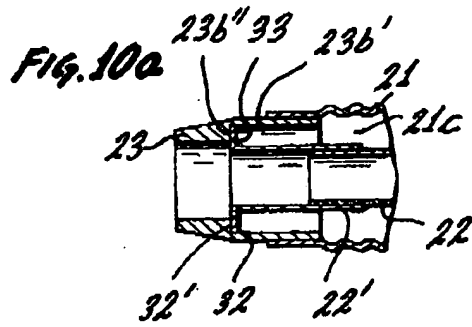
Fig. 9b



Scott & Aylor

1133350

8-5



Scott & Sylen

1133350

8-6

Fig. 12

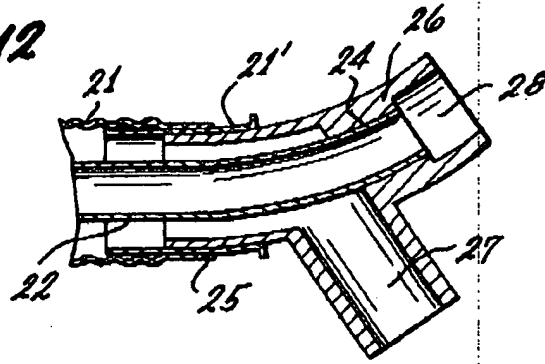
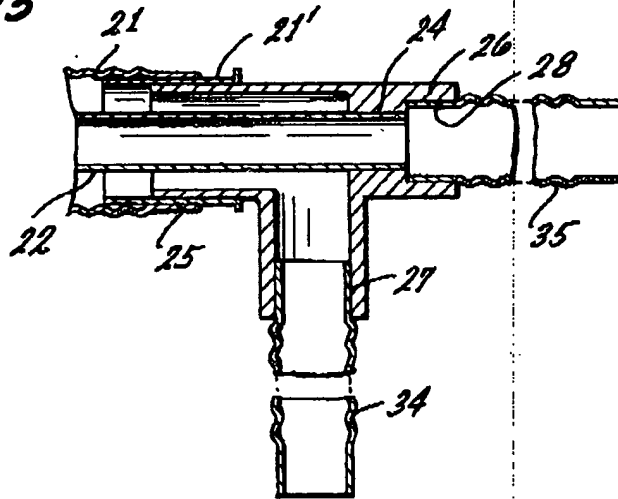


Fig. 13



Scott & Syllon

1133350

8-7

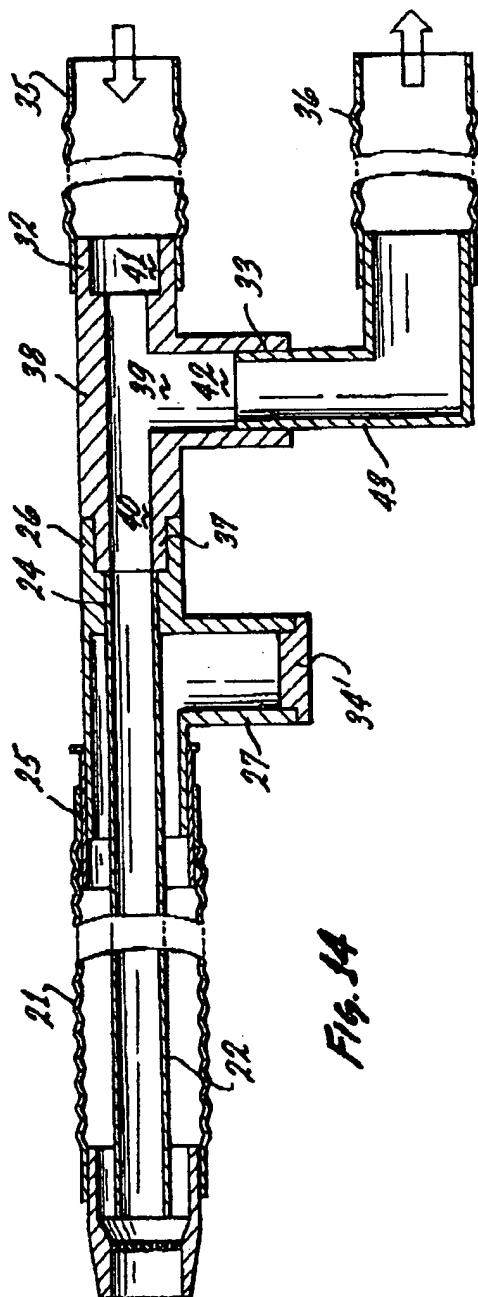


Fig. 14

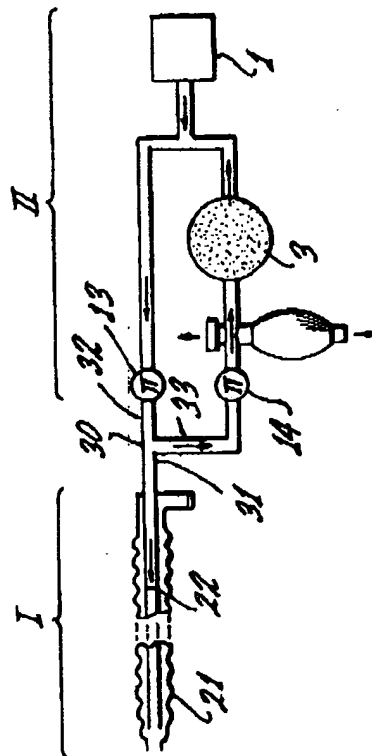


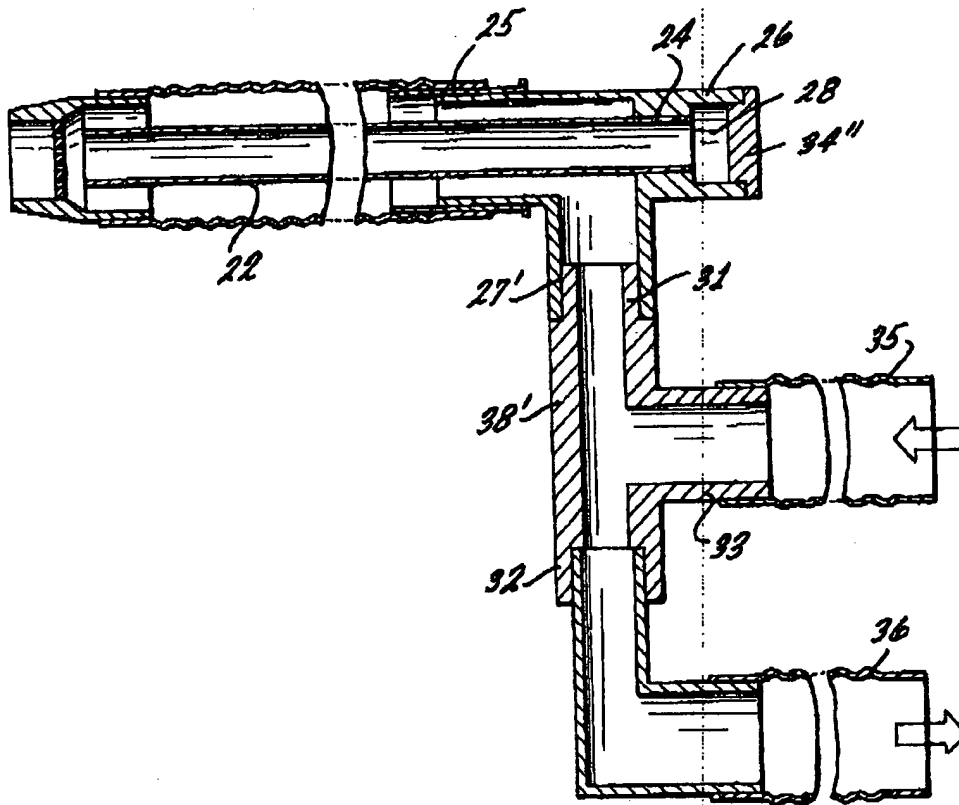
Fig. 15

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1133350

8-8

FIG. 16



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